



LOCALLY ORDERLESS REGISTRATION OF DIFFUSION WEIGHTED IMAGES

Jensen H. G.¹ (henne@di.ku.dk), Nielsen M.¹, Lauze F.¹, & Darkner S.¹

¹Image Group, Department of Computer Science, UCPH.

Abstract

Registration of Diffusion Weighted Images (DWI) is challenging as the data is a composition of both directional and intensity information. In this work, the density estimation framework for image similarity, Locally Orderless Registration, is extended to include directional information. **We construct a spatio-directional scale-space formulation of marginal and joint density distributions between two DWI.** We examine the scale-space and illustrate the approach by affine registration.

LOR

The LOR framework defines the similarity over 3 scales: The *image* scale, the *intensity* scale, and the *integration* scale.

Image scale

Given an image I , the first scale is the convolution with a kernel K_σ of standard deviation σ

$$I_\sigma(x) = (I * K_\sigma)(x) = \int_{\Omega} I(\tau) K_\sigma(x - \tau) d\tau \quad (1)$$

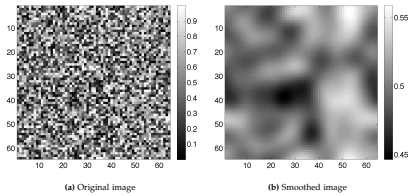


Figure 1: (Image scale) Examples of simple gaussian image smoothing.

Intensity and integration scale

To align two images I_σ and J_σ (1) under a transformation ϕ , we write up their joint histogram h . The intensity scale is essentially the soft bin width β of the histogram while the integration scale is a Gaussian integration window used to create a local histogram around x with standard deviation α .

$$h_{\beta\alpha\sigma}(i, j | \phi, x) = \int_{\Omega} \overbrace{P_{\beta}(I_{\sigma}(\phi(x)) - i)}^{\text{Intensity scale}} \overbrace{P_{\beta}(J_{\sigma}(x) - j)}^{\text{Integration scale}} \overbrace{W_{\alpha}(\tau - x)}^{\text{Integration scale}} d\tau \quad (2)$$

Here P_{β} is a Parzen-window, and W_{α} is a Gaussian integration window. This is a scale-space representation of intensity distributions in images and lets us use a set of generalized linear and non-linear similarity measures, such as Mutual Information (MI).

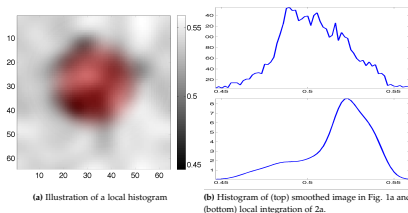


Figure 2: (Integration scale) Illustration of local integration.

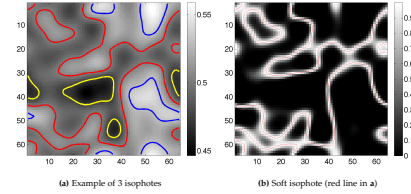


Figure 3: (Intensity scale) Examples of isophotes (i.e. bins in the histogram). 3a illustrates 3 bins while 3b shows the effect of smoothing a bin.

LOR-DWI

DWI are highly sensitive so invariant similarity measures (e.g. MI) are attractive. However, density estimation is complicated by directional information.

Adding the orientation scale

We get an *orientational* scale by adding an antipodally symmetric kernel Γ_k , and substitute the image model in (1) to encompass a vector v on the spherical domain S^2

$$I_{\sigma k}(x, v) = (I * (K_{\sigma} \otimes \Gamma_k))(x, v) = \int_{S^2} \left(\int_{\Omega} I(\tau, v) K_{\sigma}(\tau - x) d\tau \right) \Gamma_k(v, v) dv \quad (3)$$

We set Γ_k to be a Watson distribution with concentration parameter k .

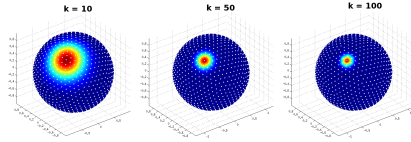


Figure 4: (Orientation scale) Example of a Watson distribution of varying support.

Now, let $\phi(x)$ be a diffeomorphic transformation of a point x , $\psi(v) = \frac{d\phi(v)}{d\phi(v)}$ be a deformation of the orientation v (based on the Jacobian of ϕ), and the overall transformation be $\tilde{\Phi} : (x, v) \mapsto (\phi(x), \psi(v))$. Updating the formulation of (2) with (3), we get the joint histogram

$$h_{\beta\alpha\sigma k}(i, j | \tilde{\Phi}, x) = \int_{\Omega \times S^2} P_{\beta}(I_{\sigma k}(\phi(x), \psi(v)) - i) P_{\beta}(J_{\sigma k}(x, v) - j) W_{\alpha}(\tau - x) d\tau \times dv \quad (4)$$

and from this, the normalized density estimate

$$p_{\beta\alpha\sigma k}(i, j | \tilde{\Phi}, x) \approx \frac{h_{\beta\alpha\sigma k}(i, j | \tilde{\Phi}, x)}{\int_{\Omega \times S^2} h_{\beta\alpha\sigma k}(i, j | \tilde{\Phi}, x) d\tau dk} \quad (5)$$

The marginal probabilities are trivially derived, and from this we can use linear (sum of squared differences, Huber, ...) and non-linear measures (MI, NMI, ...) for image registration.

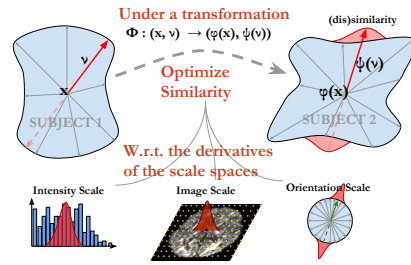


Figure 5: 2D illustration of a vector in a DWI shell (subject 1) being compared with another shell (subject 2). We calculate the derivatives of the diffeomorphic transformation w.r.t. the similarity over the smoothed scale spaces.

Experiments & Results

We performed a non-rigid registration of 2 high angular DWI scans (HARDI) from the Human Connectome Project (single shell, $b=1000$). We show that, even without any regularization term, the inherent information in the micro-structure adds its own regularization. The acquired DWI were pre-registered spatially to an MNI152 template, no global affine transformation was performed, and 30 (out of 90) gradient directions were used. Below, Figure 6 and 7 show an axial and a coronal slice from the registration. The images are the interpolated mean diffusivity.

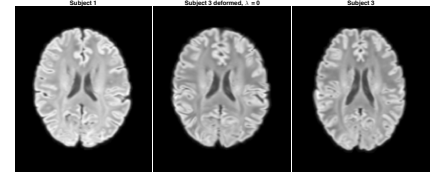


Figure 6: Interpolated mean diffusivity (axial slice). To the right (Subject 1) is the source image that the left target image (Subject 3) is registered to. The center image shows the non-rigid transformation of the target image.

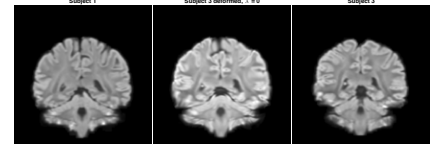


Figure 7: Interpolated mean diffusivity (coronal slice). Same as in Figure 6.

Benefits of LOR-DWI?

We extended the LOR density estimation framework to DWI. Our LOR-DWI framework allows us

- **Explicit control over the 4 scales of DWI (image scale, intensity scale, integration scale, and orientation scale).**

The scale-space formulation enables us to

- **Compare DWI across different resolutions.**

By adding a symmetric kernel on the sphere and including the first-order information of the diffeomorphic deformation, we

- **Account for the local geometrical transformation prior to modelling the distribution.**

Invariant similarity measures a key to handling the sensitive DWI scans and using our framework we can

- **Project complex DWI structures down to a 2D density estimate that enables the use of well-defined similarity measures, such as Mutual Information.**

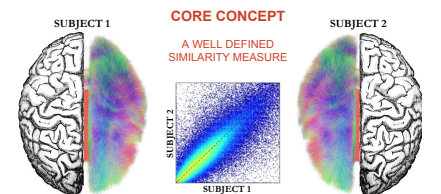


Figure 8: Illustration of two complex DWI structures projected down to a 2D density estimate using LOR-DWI.